

Radiosynthesis of ^{11}C -phenytoin Using a DEGDEE Solvent for Clinical PET Studies

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ABSTRACT

Objective(s): Phenytoin is an antiepileptic drug that is used worldwide. The whole-body pharmacokinetics of this drug have been extensively studied using ^{11}C -phenytoin in small animals. However, because of the limited production amounts that are presently available, clinical ^{11}C -phenytoin PET studies to examine the pharmacokinetics of phenytoin in humans have not yet been performed. We aimed to establish a new synthesis method to produce large amounts of ^{11}C -phenytoin to conduct human studies.

Methods: [^{11}C] methane was produced using an in-house cyclotron by the ^{14}N (p, α) ^{11}C nuclear reaction of 5 % of hydrogen containing 95 % of nitrogen gas. About 30 GBq of ^{11}C -methane was then transferred to a homogenization cell containing Fe_2O_3 powder mixed with Fe granules heated at 320 °C to yield ^{11}C -phosgene. Xylene, 1,4-dioxane, and diethylene glycol diethyl ether (DEGDEE) were investigated as possible reaction solvents.

Results: The ratio of ^{11}C -phenytoin radioactivity to the total ^{11}C radioactivity in the reaction vessel (reaction efficiency) was 7.5% for xylene, 11% for 1,4-dioxane, and 37% for DEGDEE. The synthesis time was within 45 min from the end of bombardment until obtaining the final product. The radioactivity produced was more than 4.1 GBq in 10 mL of saline at the end of synthesis. The specific activity of the product ranged from 1.7 to 2.2 GBq/ μmol . The quality of the [^{11}C] phenytoin injection passed all criteria required for clinical use.

Conclusion: The use of DEGDEE as a solvent enabled the production of a large amount of ^{11}C -phenytoin sufficient to enable PET studies examining the human pharmacokinetics of phenytoin.

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Introduction

Phenytoin is a well-characterized and widely used anti-epileptic drug (1-3). Phenytoin is a voltage-dependent Na^+ channel blocker that suppresses the excitation of neurons. In the past, the distribution of ^{11}C -labeled phenytoin and its derivatives has been studied using positron emission tomography (PET) in animals and humans. Meldrum et al. synthesized ^{11}C -hydantoin analogs, including ^{11}C -phenytoin, using ^{11}C -HCN (4). In their study, the radioactivity of the ^{11}C -phenytoin was 74 MBq at the time of injection, and the total synthesis time was 106 min. Stavchansky et al. and Emaran et al. produced ^{11}C -hydantoin analogs from ^{11}C -HCN using different precursors (5, 6). Roeda et al. synthesized ^{11}C -phenytoin from ^{11}C -phosgene (7). In these previous studies, however, the difficulty of producing a stable and large amount of ^{11}C -phenytoin restricted the clinical use of ^{11}C -phenytoin for measuring the whole-body distribution. We previously reported an ^{11}C -phenytoin kinetic study in small animals where only small amounts of ^{11}C -phenytoin (5 MBq) were used (8). In the previous report, we did not describe the details of synthesis methods. Baron et al. reported ^{11}C -phenytoin accumulation in the human brain (9). Although ^{11}C -phenytoin PET was expected to be a useful tool for pharmacokinetic studies of phenytoin and a biomarker of voltage-dependent Na^+ channel distribution and density in humans, other researchers have not pursued this potential because of the difficult radiosynthesis method.

The purpose of the present study was to establish a synthesis method for ^{11}C -phenytoin suitable for clinical use. A large amount of radioactivity (at least 370 MBq) at the time of injection and a high level of safety were required. In this study, we investigated various reaction conditions for ^{11}C -phenytoin, especially the selection of a reaction solvent.

Methods

Chemicals

The precursor of ^{11}C -phenytoin, 2-amino-2,2-diphenylacetamide, was provided by Dainippon Seiyaku Co., Ltd. (Osaka, Japan). Phenytoin was purchased from Wako Pure Chemical Co., Ltd. (Osaka, Japan). Other chemicals and solvents were purchased as follows: iron granules (10–40 mesh, 99.999%) from Aldrich Chemical Co., Milwaukee, WI; iron (III) oxide powder (98.0%) and chlorine gas (99.999%) from Asahi Denka

Kogyo K.K., Tokyo, Japan; and antimony powder (99.8%) from Merck KGaA., Darmstadt, Germany. These reagents were used without further purification.

Synthesis of ^{11}C -phosgene

^{11}C -phosgene was produced according to a method previously reported by Nishijima et al. (10). Briefly, ^{11}C -methane was produced using an in-house cyclotron (CYPRIS-HM18, Sumitomo Heavy Industries, Tokyo, Japan) by a $^{14}\text{N}(\text{p}, \alpha)^{11}\text{C}$ nuclear reaction on 5 % of hydrogen containing 95 % of nitrogen gas. The irradiation conditions were a 10–15 μA proton beam for 40–60 min at 18 MeV. An automated synthesis apparatus (CUPID, Sumitomo Heavy Industries) was used for the radiolabeling of ^{11}C -phosgene (Figure 1). About 40 GBq of ^{11}C -methane produced in the target box was trapped and condensed in a stainless U-tube (4 mm; I.D., 150 mm) immersed in liquid nitrogen and filled with Porapak Q (80–100 mesh; Waters, Milford, MA). The stainless U-tube was then warmed to room temperature. The ^{11}C methane within the stainless U-tube was transferred by helium flow to the first homogenization cell (glass-Teflon gas-tight syringe). 2 ml of chlorine gas was added to the first homogenization cell by gas tight syringe. Then the first homogenization cell was heated at 560 $^{\circ}\text{C}$. In this step, ^{11}C -methane was converted to ^{11}C carbon tetrachloride ($^{11}\text{C}\text{-CCl}_4$). $^{11}\text{C}\text{-CCl}_4$ was transferred to the second homogenization cell filled with Fe_2O_3 powder and Fe granules (1.5 g; Fe_2O_3 powder/Fe granules, 1/28, w/w). The second homogenization cell was heated at 320 $^{\circ}\text{C}$ to yield ^{11}C phosgene. Finally, the ^{11}C -phosgene was passed through an antimony column to remove chlorine.

Investigation of reaction solvents

Xylene, 1,4-dioxane, and diethylene glycol diethyl ether (DEGDDE) were investigated as possible reaction solvents. The precursor of ^{11}C -phenytoin was dissolved in each solvent. ^{11}C -phosgene was then bubbled in a reaction vessel containing each solvent. The reaction vessel was then heated to a temperature near boiling (140 $^{\circ}\text{C}$ for xylene, 100 $^{\circ}\text{C}$ for 1,4-dioxane, and 180 $^{\circ}\text{C}$ for DEGDDE) for 10 min.

Synthesis of ^{11}C -phenytoin injection

About 30 GBq of ^{11}C -phosgene was introduced to a reaction vessel containing 4 mg of 2-amino-2,2-diphenylacetamide in 2.0 mL of DEGDDE and

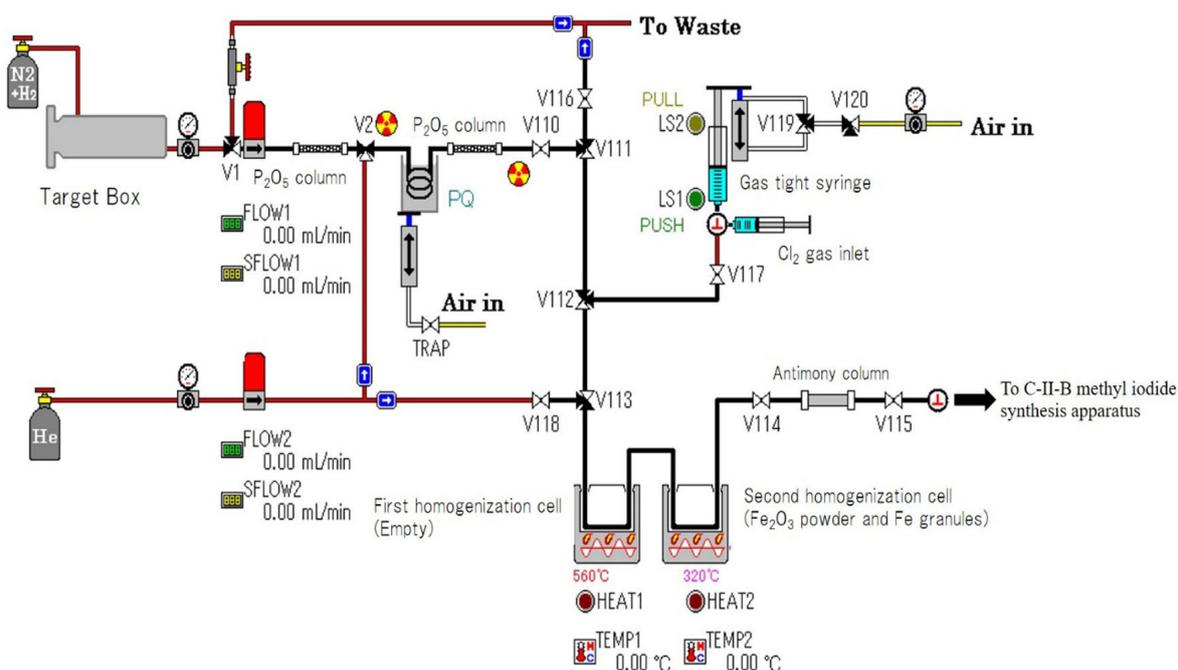


Figure 1. Diagram of an automated synthesis apparatus for ¹¹C-phenytoin

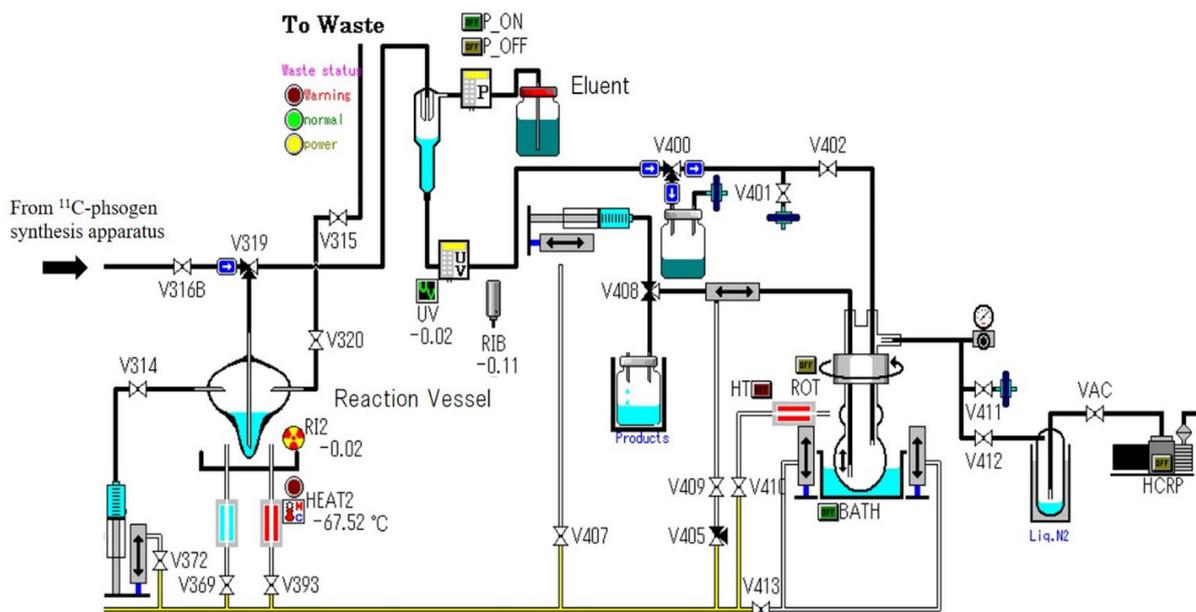


Figure 2. Diagram of C-II-B methyl iodide synthesis apparatus

set in a C-II-B methyl iodide synthesis apparatus (Figure 2 and Figure 3), with 200 mL/min of helium gas. Then, the reaction mixture was heated to 180 °C for 10 min. The reaction was quenched by the addition of 2.5 % ammonia solution and ethanol mixture (25/75, v/v). The

reaction mixture was transferred to an HPLC system. The HPLC separation conditions were as follows: a YMC-pack polymer C18 column (10 mm × 250 mm; YMC, Kyoto, Japan), a separation eluent consisting of 2.5 % ammonia solution and ethanol (25/75, v/v), and a flow rate of 2.0 mL/min. The

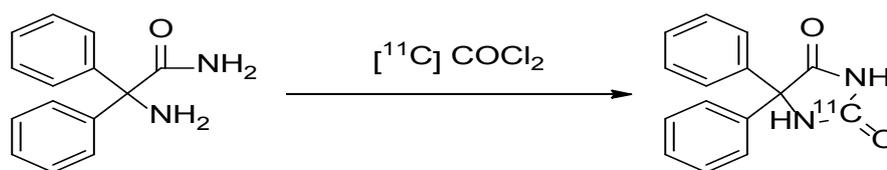


Figure 3. Synthesis route of ^{11}C -phenytoin

retention time of ^{11}C -phenytoin was 8 min.

After HPLC separation, 100 mL of the ^{11}C -phenytoin fraction was collected in a recovery flask. The solvent was removed by evaporation. The residue was resolved using saline. The final product was sterilized by filtration using a Millex-GV filter (Merck Millipore, Darmstadt, Germany).

Quality control for ^{11}C -phenytoin injections

The items examined for quality control were pH, color and particles in injection solution, radionuclide impurities, radiochemical purity, physical half-life, endotoxin test, sterilization test, and residual amount of ammonium ion, ethanol, and DEGDEE in the injection solution. Radiochemical purity and specific activity of ^{11}C -phenytoin were measured by analytical HPLC. Analytical HPLC was performed using a Polymer C18 column and 50 mM Na_3PO_4 + 5 mM sodium dodecyl sulfate/acetonitrile (60/40, v/v). We confirmed that the major radioactivity is ^{11}C -phenytoin with analytical HPLC. The retention time is corresponding with that of non-radioactive standard. Specific activity of ^{11}C -phenytoin is calculated from total amount of phenytoin. Amount of phenytoin was determined from UV absorption calibration curve of non-radioactive phenytoin analysis. The ammonia concentration was measured using Fuji Dry Chem 100 and Fuji Dry Chem slide NH_3 -PII (Fuji Film Medical, Tokyo, Japan). The ethanol and DEGDEE concentrations were measured using gas chromatography (GC-14B; Shimadzu, Kyoto, Japan). For ethanol, a TSG-1 15 % SHINCARBON A 60/80 3.2×3.3 , 100 mm column was used (Shimadzu, Kyoto, Japan). The column temperature was 90 °C. A Flame Ionization Detector was used. The detector temperature was 180 °C. The carrier gas was nitrogen, and the flow rate was 30 mL/min. Under these conditions, ethanol was detected at 4 min. For DEGDEE, a G-300 40 m \times 1.2 mm column was used (Chemicals Evaluation and Research Institute, Japan, Tokyo, Japan). The column temperature

was 130 °C. A Flame Ionization Detector was used. The detector temperature was 180 °C. The carrier gas was helium, and the flow rate was 30 mL/min. Under these conditions, DEGDEE was detected at 4.5 min.

The quality control of the ^{11}C -phenytoin product was validated according to the criteria of the Safety Control Committee for Short-lived Radiopharmaceuticals, Osaka University Hospital.

Results

Comparison among reaction solvents

The ratio of ^{11}C -phenytoin radioactivity to the total ^{11}C radioactivity in the reaction vessel (reaction efficiency) was 7.5 % for xylene, 11.0 % for 1,4-dioxane, and 37.0 % for DEGDEE. Because DEGDEE had the highest reaction efficiency among these three solvents, the synthesis and quality control of ^{11}C -phenytoin was studied using DEGDEE.

Synthesis of ^{11}C -phenytoin solution

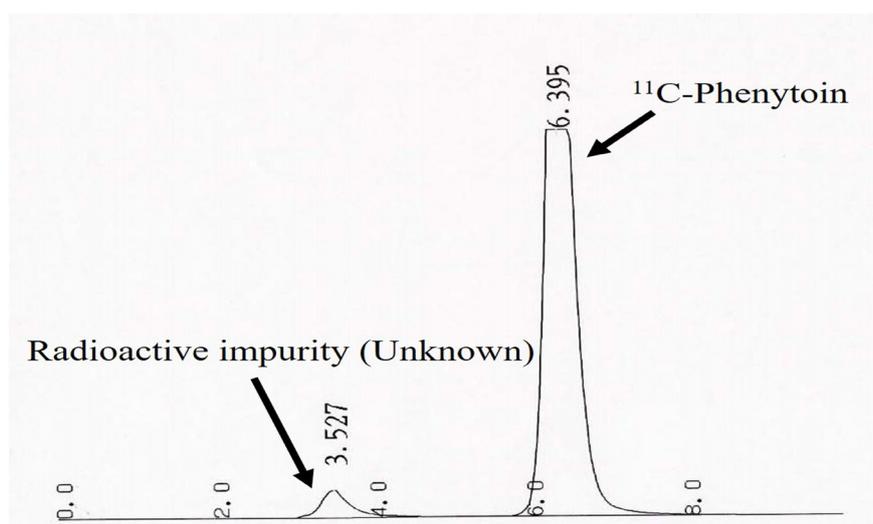
The synthesis time was within 45 min from the end of bombardment to the final product. The radioactivity produced was more than 4.1 GBq at the end of synthesis (Table 1).

Quality control for ^{11}C -phenytoin solution

^{11}C -phenytoin was produced three times. The total procedure for quality control was completed within 20 min. The results of the quality control and the criteria of the Safety Control Committee for Short-lived Radiopharmaceuticals, Osaka University Hospital, are shown in Table 1. All the samples were clear and colorless by visual inspection. No particles were visually detected. No bacterial colonies were detected two weeks after the study. The values for specific activity, pH, radionuclide impurities, radiochemical purity, physical half-life, and amount of ammonium ion, ethanol, and DEGDEE were within the ranges of the quality control criteria. The HPLC chromatogram of radiochemical purity measurement is shown in Figure 4.

Table 1. Results of ^{11}C -phenytoin synthesis and quality control criteria

	Run 1	Run 2	Run 3	Criterion value
Radioactivity (EOS)	6.2 GBq	7.9 GBq	4.1 GBq	-----
Radioactivity for Injection	3.1 GBq	3.5 GBq	2.0 GBq	
Specific activity	1.9 GBq/ μmol	2.2 GBq/ μmol	1.7 GBq/ μmol	>1.0 GBq/ μmol
pH	6.3–6.9	6.3–6.9	6.3–6.9	5.0–8.0
Color	Clear and colorless	Clear and colorless	Clear and colorless	Clear and colorless
Particles	None	None	None	None
Radionuclide impurities	511 keV only	511 keV only	511 keV only	511 keV only
Radiochemical purity	>95%	>95%	>95%	>95%
Half-life	20.3 min	20.0 min	20.4 min	19-21 min
Endotoxin test	Pass	Pass	Pass	<0.25 EU/mL
Sterilization test	Pass	Pass	Pass	Pass
Ammonium ion	91 $\mu\text{g}/\text{dL}$	17 $\mu\text{g}/\text{dL}$	46 $\mu\text{g}/\text{dL}$	200 $\mu\text{g}/\text{dL}$
Ethanol	<10 ppm	<10 ppm	<10 ppm	<2000 ppm
DEGDEE	<10 ppm	<10 ppm	<10 ppm	<100 ppm

**Figure 4.** Radio-HPLC chart of ^{11}C -phenytoin for radiochemical purity analysis

Discussion

Roeda et al. reported the use of xylene for the synthesis of ^{11}C -phenytoin (7). Their study indicated that the use of xylene as a solvent resulted in a high reaction efficiency of around 70 %. However, in the present study, the reaction efficiency was only 7.5 %. In addition, xylene must be removed before HPLC purification because of its high lipophilicity. Because of the low reaction efficiency and long synthesis time, we concluded that xylene was not an appropriate solvent for ^{11}C -phenytoin production for use in clinical PET

studies.

We selected the water-soluble solvents 1,4-dioxane and DEGDEE to avoid the need for a solvent removal procedure prior to HPLC purification. The synthesis time was within 45 min when these solvents were used. The reaction efficiencies were 10 % and 37 % for 1,4-dioxane and DEGDEE, respectively. Therefore, we selected DEGDEE as a solvent for the production of large amounts of ^{11}C -phenytoin for use in clinical PET studies.

The European Union and USA authorities have recommended the use of human PET studies with labeled candidate compounds during the early phase of new drug development (EU, USA) (11, 12). Our previous study of ¹¹C-donepezil indicated that the whole-body absorption, distribution, metabolism, and excretion of clinically prescribed medicines can be evaluated in humans using PET (13). In such studies, the mass dose of the tracer was limited to 100 mg or less with adequate radioactivity for imaging according to the recommendations by EU and USA authorities (EU, USA). In the present study, the specific activity of ¹¹C-phenytoin after quality control was 1.9, 2.2, and 1.7 GBq/μmol. These activities corresponded to 750, 870, and 670 MBq/100 mg at the time of injection. In recent clinical PET studies with currently available scanners using ¹¹C labeled tracers such as ¹¹C-methionine, the injection dose is approximately 3 MBq/kg, or around 200 MBq/body (14). Therefore, the current synthesis method for ¹¹C-phenytoin provides sufficient radioactivity with a tracer amount of less than 100 mg. Optimization of the labeling procedure, reagents, and quality control should be further investigated in the future.

Conclusion

The use of DEGDEE as a solvent enabled the production of a large amount of ¹¹C-phenytoin solution with a high specific activity sufficient to enable PET studies examining the human pharmacokinetics of phenytoin.

References

- Buchthal F, Svensmark O, Schiller PJ. Clinical and electroencephalographic correlations with serum levels of diphenylhydantoin. *Arch Neurol*. 1960;2(6):624-30.
- Noach EL, Woodbury DM, Goodman LS. Studies on the absorption, distribution, fate and excretion of 4-C¹⁴-labeled diphenylhydantoin. *J Pharmacol Exp Ther*. 1958;122(3):301-14.
- Noach EL, Vanrees HV. Intestinal distribution of intravenously administered diphenylhydantoin in the rat. *Arch Int Pharmacodyn Ther*. 1964; 150:52-61.
- Winstead MB, Parr SJ, Rogal MJ, Brockman PS, Lubcher R, Khentigan A, et al. Relationship of molecular structure to in vivo scintigraphic distribution patterns of carbon-11-labeled compound. 3. [¹¹C] hydantoins. *J Med Chem*. 1976;19(2):279-86.
- Stavchansky SA, Tilbur RS, McDonald JM, Ting CT, Kostenbauder HB. In vivo distribution of carbon-11 phenytoin and its major metabolite, and their use in scintigraphic imaging. *J Nucl Med*. 1978;19(8):936-41.
- Emran AM, Boothe TE, Finn RD, Vora MM, Kothari PJ. Use of ¹¹C as a tracer for studying the synthesis of radiolabelled compounds-II: 2-[¹¹C]-5, 5-diphenylhydantoin from [¹¹C] cyanide. *Int J Radiat Appl Instrument A*. 1986;37(10):1033-8.
- Roeda D, Westera G. The synthesis of some ¹¹C-labeled antiepileptic drugs with potential utility as radiopharmaceuticals: hydantoins and barbiturates. *Int J Appl Radiat Isotopes*. 1981;32(11):843-5.
- Hasegawa Y, Kanai Y, Hasegawa S, Okamoto T, Matsui T, Shimosegawa E, et al. Evaluation of brain and whole-body pharmacokinetics of ¹¹C-labeled diphenylhydantoin in rats by means of planar positron imaging system. *Ann Nucl Med*. 2008;22(4):301-7.
- Baron JC, Roeda D, Munari C, Crouzel C, Chodkiewicz JP, Comar D. Brain regional pharmacokinetics of ¹¹C-labeled diphenylhydantoin: positron emission tomography in humans. *Neurology*. 1983;33(5):580-5.
- Nishijima K, Kuge Y, Seki K, Ohkura K, Motoki N, Nagatsu K, et al. A simplified and improved synthesis of [¹¹C]phosgene with iron and iron (III) oxide. *Nucl Med Biol*. 2002;29(3):345-50.
- EU/EMA/CPMP: position paper on non-clinical safety studies to support clinical trials with a single microdose. London: The European Medicines Agency (EMA), Evaluation of Medicines for Human Use, CPMP/SWP/2599/02; 2003.
- FDA US. Guidance for industry, investigators and reviewers, exploratory IND studies, US Department of Health and Human Services. New York: FDA, CDER; 2006
- Mochida I, Shimosegawa E, Kanai Y, Naka S, Matsunaga K, Isohashi K, et al. Whole-body distribution of donepezil as an acetylcholinesterase inhibitor after oral administration in normal human subjects: a ¹¹C-donepezil PET study. *Asia Ocean J Nucl Med Biol*. 2017;5(1):3-9.
- Takano K, Kinoshita M, Arita H, Okita Y, Chiba Y, Kagawa N, et al. Diagnostic and prognostic value of ¹¹C-methionine PET for nonenhancing gliomas. *Am J Neuroradiol*. 2016;37(1):44-50.