

Performance of Myocardial Perfusion Imaging Using Multi-focus Fan Beam Collimator with Resolution Recovery Reconstruction in a Comparison with Conventional SPECT

Norikazu Matsutomo^{1, 2*}, Akio Nagaki¹, Masayuki Sasaki²

¹ Department of Radiology, Kurashiki Central Hospital, Kurashiki, Japan

² Department of Health Sciences, Graduate School of Medical Sciences, Kyushu University, Fukuoka, Japan

ARTICLE INFO

Article type:

Original article

Article history:

Received: 2 Apr 2014

Revised: 14 May 2014

Accepted: 16 May 2014

Keywords:

Multi-focus fan beam collimator
Myocardial perfusion imaging
Comparable images
Resolution recovery reconstruction

ABSTRACT

Objective(s): IQ-SPECT is an advanced high-speed SPECT modality for myocardial perfusion imaging (MPI), which uses a multi-focus fan beam collimator with resolution recovery reconstruction. The aim of this study was to compare IQ-SPECT with conventional SPECT in terms of performance, based on standard clinical protocols. In addition, we examined the concordance between conventional and IQ-SPECT in patients with coronary artery disease (CAD).

Methods: Fifty-three patients, undergoing rest-gated MPI for the evaluation of known or suspected CAD, were enrolled in this study. In each patient, conventional SPECT (^{99m}Tc-tetrofosmin, 9.6 min and ²⁰¹Tl, 12.9 min) was performed, immediately followed by IQ-SPECT, using a short acquisition time (4.3 min for ^{99m}Tc-tetrofosmin and 6.2 min for ²⁰¹Tl). A quantitative analysis was performed on an MPI polar map, using a 20-segment model of the left ventricle. An automated analysis by gated SPECT was carried out to determine the left ventricular volume and function including end-diastolic volume (EDV), end-systolic volume (ESV), and left ventricular ejection fraction (LVEF). The degree of concordance between conventional SPECT and IQ-SPECT images was evaluated according to linear regression and Bland-Altman analyses.

Results: The segmental percent uptake exhibited a significant correlation between IQ-SPECT and conventional SPECT ($P < 0.05$). The mean differences in ^{99m}Tc-tetrofosmin studies were $1.1 \pm 6.6\%$ (apex), $2.8 \pm 5.7\%$ (anterior wall), $2.9 \pm 6.2\%$ (septal wall), $4.9 \pm 6.7\%$ (lateral wall), and $1.8 \pm 5.6\%$ (inferior wall). Meanwhile, regarding the ²⁰¹Tl-SPECT studies, these values were $1.6 \pm 6.9\%$, $2.0 \pm 6.6\%$, $2.1 \pm 5.9\%$, $3.3 \pm 7.2\%$, and $2.4 \pm 5.8\%$, respectively. Although the mean LVEF in IQ-SPECT tended to be higher than that observed in conventional SPECT (conventional SPECT = $64.8 \pm 11.8\%$ and IQ-SPECT = $68.3 \pm 12.1\%$ for ^{99m}Tc-tetrofosmin; conventional SPECT = $56.0 \pm 11.7\%$ and IQ-SPECT = $61.5 \pm 12.2\%$ for ²⁰¹Tl), quantitative parameters were not significantly different between IQ-SPECT and conventional SPECT.

Conclusion: According to the ^{99m}Tc-tetrofosmin and ²⁰¹Tl protocols, IQ-SPECT images were comparable to and in agreement with conventional SPECT images. Our results suggest that IQ-SPECT is a useful technology for MPI SPECT, and can lead to an increase in scan efficiency and patient comfort.

► Please cite this paper as:

Matsutomo N, Nagaki A, Sasaki M. Performance of Myocardial Perfusion Imaging Using Multi-focus Fan Beam Collimator with Resolution Recovery Reconstruction in a Comparison with Conventional SPECT. Asia Oceania J Nucl Med Biol. 2014; 2(2):111-119.

Introduction

Myocardial perfusion imaging (MPI) is currently the most widely performed imaging modality for the diagnosis of ischemic heart

disease (1-5). However, MPI requires a relatively long acquisition time for securing sufficient image quality for clinical purposes. In

* Corresponding author: Norikazu Matsutomo, Department of Radiology, Kurashiki Central Hospital, 1-1-1 Miwa, Kurashiki, Okayama, 710-8602, Japan. Tel: +81-86-422-0210; Fax: +81-86-421-3424; Email: nm7074@kchnet.or.jp

© 2014 mums.ac.ir All rights reserved.

This is an Open Access article distributed under the terms of the Creative Commons Attribution License (<http://creativecommons.org/licenses/by/3.0>), which permits unrestricted use, distribution, and reproduction in any medium, provided the original work is properly cited.

addition, long acquisition time results in image artifacts (e.g., motion artifacts), particularly in severely ill or older patients.

Advances in MPI technology have provided an opportunity for improved image quality, patient comfort, and throughput. In this regard, Asao et al. (6) reported that the interpolated projection data estimation processing (IPDE) method improves the image quality of MPI single-photon emission computerized tomography (SPECT), given the short acquisition time.

Borges-Neto et al. (7), Sun et al. (8), and Venero et al. (9) showed that a reconstruction algorithm, employing collimator distance-dependent resolution recovery, is expected to have the potential to decrease the acquisition time and improve diagnostic accuracy. However, these results were simply due to the effects of image processing and/or application of resolution recovery method; in fact, the findings were not associated with acquisition count.

The most basic factor required to obtain good image quality, using SPECT, is the acquired count since SPECT image quality is determined by signal-to-noise ratio. Therefore, development of a new SPECT system for obtaining a high acquisition count is required to acquire high quality images.

IQ-SPECT (Siemens AG, Erlangen, Germany) is a recently developed and advanced high-sensitivity SPECT technology that is expected to improve the efficiency of MPI. IQ-SPECT consists of three advanced features including a multi-focus fan beam collimator, cardio-centric acquisition and three-dimensional reconstruction with collimator geometry (10).

The multi-focus fan beam collimator is designed in a way that the center of the field of view magnifies the heart. In addition, the collimator varies similar to a cone beam in the center, parallel to the edges; this structure contributes to the ability of collimator to increase the count. The cardio-centric imaging device rotates around a center of rotation,

positioned in the heart (in a highly sensitive area of the collimator). The IQ reconstruction algorithm takes into account the unique position and shape of the collimator holes as well as the orientation of the detectors. Therefore, IQ-SPECT images are routinely reconstructed with resolution recovery and geometric correction of multi-focus collimator.

These unique features have the potential to increase the photon-sensitivity with no associated loss of resolution. Our group has previously reported that IQ-SPECT significantly improved image resolution and quality, compared to conventional SPECT in various physical phantom studies (11). However, the image accuracy and performance of IQ-SPECT has not been clinically examined yet.

In the present study, we compared IQ-SPECT with conventional SPECT in terms of performance, based on standard clinical protocols. In addition, we examined the concordance between IQ-SPECT images and conventional SPECT images in patients with coronary artery disease (CAD).

Methods

Patient population

Fifty-three patients (38 males and 15 females) with the mean age of 70.2 ± 11.0 years (within the range of 40-90 years), undergoing rest-gated MPI for the evaluation of known or suspected CAD, were enrolled in this study. The

Table 1. Characteristics of the patient population

	^{99m} Tc	²⁰¹ Tl
Age(y)		
Mean±SD	71.3 ± 12.1	69.7 ± 10.0
Sex		
Male	18	20
Female	7	8
Final diagnoses		
AP	13	14
OMI	6	10
unspecified IHD	6	4
History of percutaneous coronary intervention		
	12	21

AP: angina pectoris, OMI: old myocardial Infarction
IHD: ischemic heart disease

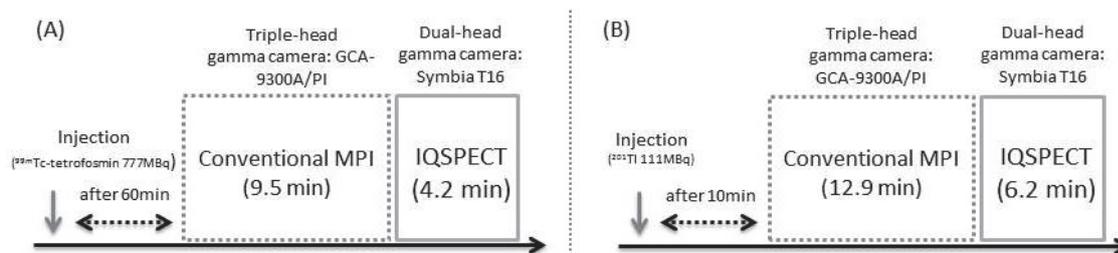


Figure 1. Schematic drawing of MPI SPECT, using ^{99m}Tc-tetrofosmin (A) and ²⁰¹Tl (B). All images were initially acquired by conventional SPECT, immediately followed by IQ-SPECT

included patients were those with a previous history of percutaneous coronary intervention or myocardial infarction. The patients' characteristics are shown in Table 1.

All patients were initially examined using conventional SPECT, followed immediately by IQ-SPECT (Figure 1). ^{99m}Tc -tetrofosmin MPI SPECT was performed on 25 patients, and ^{201}Tl SPECT was carried out on 28 patients.

For the ^{99m}Tc -tetrofosmin studies, 777 MBq of ^{99m}Tc -tetrofosmin was intravenously injected at rest, and SPECT was initiated approximately 60 min after the injection. For the ^{201}Tl studies, 111 MBq of ^{201}Tl was administered intravenously, and the imaging began 15 min after the injection.

The study protocol was approved by the local ethics committee, and informed consents were obtained from all the participants.

Conventional SPECT acquisition and reconstruction

Conventional SPECT images were acquired using a triple-head gamma camera (GCA-9300A/PI, Toshiba Medical Systems, Tokyo, Japan), equipped with a low-energy high-resolution, parallel hole collimator. The projection data were obtained using a 64×64 matrix through a 360° rotation at a step size of 6° with an acquisition time of 25 and 35 sec per projection (for ^{99m}Tc -tetrofosmin and ^{201}Tl , respectively), resulting in a total acquisition time of 9.6 min for ^{99m}Tc and 12.9 min for ^{201}Tl (including the rotation time between the successive angles).

For ^{99m}Tc -tetrofosmin, a 20% energy window was centered on 140 keV photopeak and for ^{201}Tl imaging, a 20% energy window, centered on 70 keV peak was used. All studies were electrocardiograph (ECG)-gated at eight frames per R-R interval. The SPECT images were reconstructed on a commercially available workstation, using filtered-back projection with a ramp filter. Also, the Butterworth filter (order=8, cut-off frequency of 0.45 cycle/cm) was used as a pre-processing filter. Short-axis images as well as vertical and horizontal long-axis images were acquired without attenuation or scatter correction.

IQ-SPECT acquisition and reconstruction

IQ-SPECT was performed using a dual-head gamma camera (Symbia T16, Siemens AG, Erlangen, Germany) with IQ-SPECT modifications and a multi-focus fan beam collimator (Smart Zoom).

The projection data sets were acquired over 208° cardio-centric orbits with 17 views per

detector for 9 sec (^{99m}Tc -tetrofosmin) or 14 sec per projection (^{201}Tl), resulting in a total acquisition time of 4.3 min for ^{99m}Tc and 6.2 min for ^{201}Tl (including the rotation time between the successive angles) on a 128×128 matrix.

For ^{99m}Tc -tetrofosmin, a 15% energy window was centered on 140 keV photopeak and for ^{201}Tl imaging, a 15% energy window, centered on 70 keV peak was used. All studies were ECG-gated at eight frames per R-R interval. The SPECT images were reconstructed using ordered subset conjugates-gradient minimization with 30 iterations and one subset. The reconstructed images were post-smoothed using a 3D Gaussian spatial filter (FWHM= 13 mm); neither scatter nor attenuation correction was performed.

Quantitative analysis

A quantitative analysis was performed on an MPI polar map, using a reference to 20-segment model of the left ventricle, recommended by American Society of Nuclear Cardiology. The polar map was generated using a commercially available software program (Cedars QGS/QPS, Cedars-Sinai Medical Center) (12). The myocardial uptake was normalized to the peak activity, and the relative percent uptake of each segment was determined.

We also grouped the 20 segments into five regions: apex (segments 19 and 20), anterior (segments 1, 2, 7, 8, 13, and 14), septal (segments 3, 9, and 15), lateral (segments 5, 6, 11, 12, 17, and 18) and inferior (segments 4, 10, and 16) regions. In addition, an automated analysis was performed on gated SPECT images to determine the left ventricular (LV) volume and function including the end-diastolic volume (EDV), end-systolic volume (ESV), and left ventricular ejection fraction (LVEF).

Statistical analysis

The degree of concordance between the conventional SPECT and IQ-SPECT images was evaluated using linear regression and Bland-Altman analyses. All IQ-SPECT parameters (percent uptake, EDV, ESV, and LVEF) were compared with those of conventional SPECT, using a paired t-test. P-value less than 0.05 was considered statistically significant, and confidence interval was determined as 95%.

Results

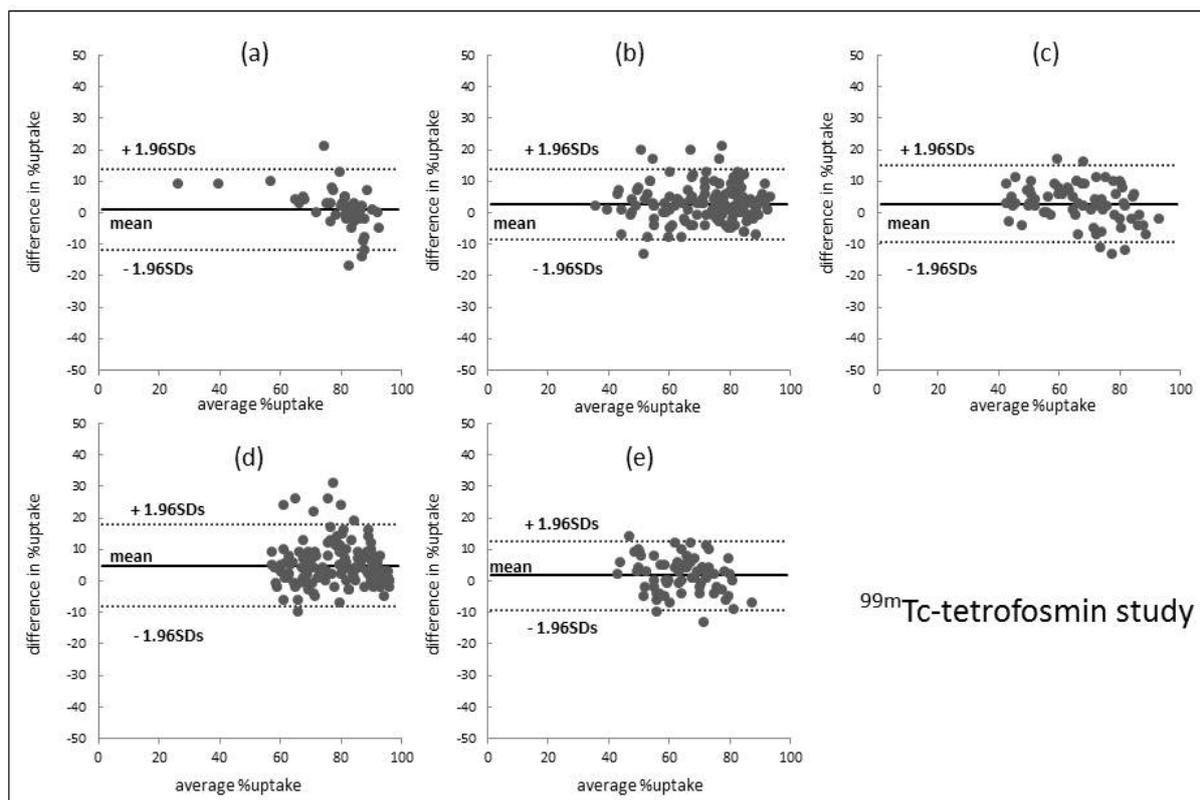
Segmental percent uptake

The interclass correlation coefficients for segmental uptake between conventional SPECT and IQ-SPECT are shown in Table 2. The interclass correlation coefficients for the ^{99m}Tc -

Table 2. Comparison of the percent segmental uptake between IQSPECT and conventional SPECT

	^{99m} Tc-tetrofosmin study			²⁰¹ Tl study		
	% uptake		Correlation coefficient	% uptake		Correlation coefficient
	Conventional SPECT	IQSPECT		Conventional SPECT	IQSPECT	
Apex	79.9±11.2	78.8±14.1	0.891	76.3±12.2	74.7±14.4	0.879
Anterior	73.6±13.6	70.8±13.6	0.912	73.4±13.5	71.3±14.0	0.885
Septal	68.4±12.2	65.5±14.6	0.906	66.7±14.6	64.6±15.2	0.922
Lateral	81.3±11.7	76.4±12.0	0.841	76.7±14.2	73.4±15.2	0.881
Inferior	65.5±9.8	67.7±11.1	0.863	64.0±13.5	61.6±13.6	0.909

Mean±SD

**Figure 2.** Bland-Altman analysis of the segmental percent uptake on IQ-SPECT and conventional SPECT in ^{99m}Tc-tetrofosmin studies. a) apex, b) anterior, c) septal, d) lateral, and e) inferior. The mean difference in the lateral wall between IQ-SPECT and conventional SPECT slightly increased

tetrofosmin segmental uptake were 0.891 (apex), 0.912 (anterior wall), 0.906 (septal wall), 0.841 (lateral wall), and 0.863 (inferior wall). Meanwhile, these values for ²⁰¹Tl segmental uptake were 0.879, 0.885, 0.922, 0.881, and 0.909, respectively (Table 2).

The percent uptake values showed no significant differences between conventional SPECT and IQ-SPECT images.

Figures 2 and 3 present the results of Bland-Altman analysis of segmental percent uptake in IQ-SPECT and conventional SPECT. The mean differences in the ^{99m}Tc-tetrofosmin studies were 1.1 ± 6.6% (apex), 2.8 ± 5.7% (anterior wall), 2.9 ± 6.2% (septal wall), 4.9 ± 6.7% (lateral wall), and 1.8 ± 5.6% (inferior wall). For the ²⁰¹Tl studies, these values were 1.6 ± 6.9%,

2.0 ± 6.6%, 2.1 ± 5.9%, 3.3 ± 7.2%, and 2.4 ± 5.8%, respectively.

There were no changes in the distribution of differences in the mean values. However, the mean difference between IQ-SPECT and conventional SPECT slightly increased in the lateral wall. Representative cases of MPI, evaluated with both IQ-SPECT and conventional SPECT, are presented in Figure 4. The perfusion defects were similar on both IQ-SPECT and conventional SPECT images.

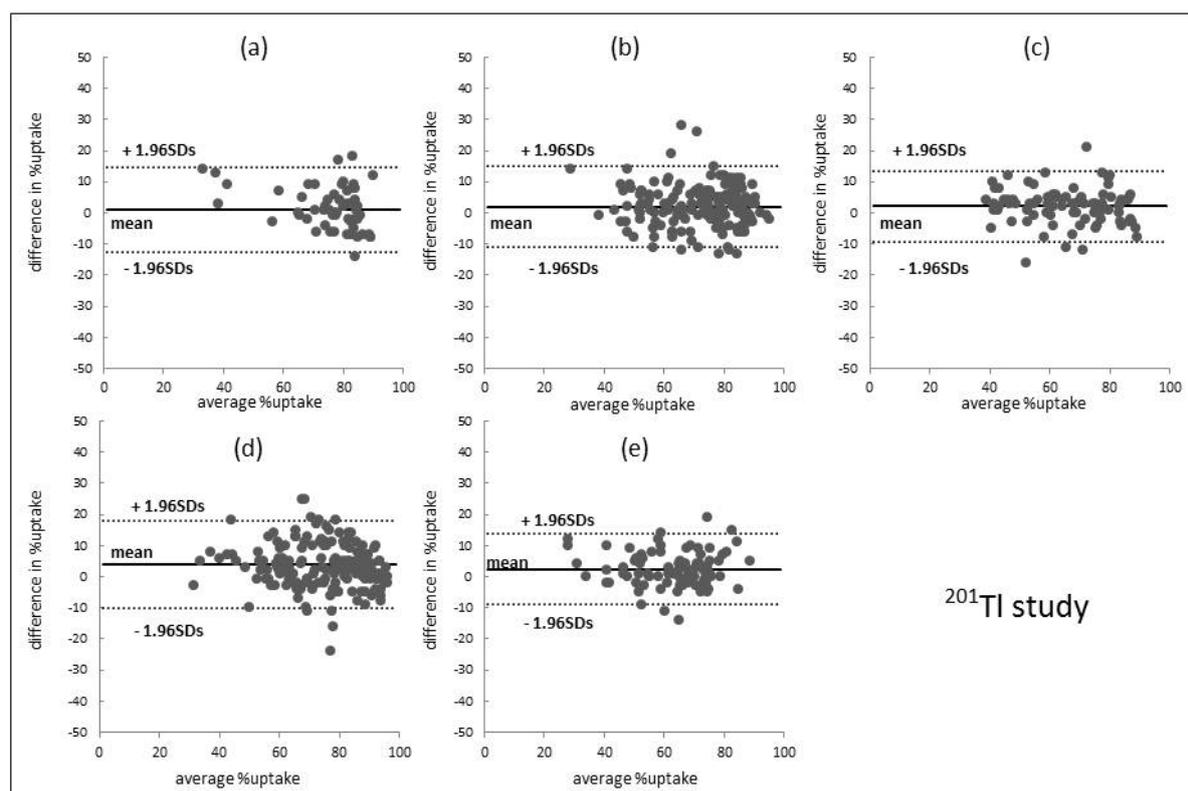
LV volume and ejection fraction

The correlations between EDV, ESV, and LVEF values on IQ-SPECT and conventional SPECT are shown in Table 3 and Figure 5. The correlation coefficients for the ^{99m}Tc-

Table 3. Comparison of the EDV, ESV, and LVEF values between IQSPECT and conventional SPECT

	^{99m} Tc-tetrofosmin study			²⁰¹ Tl study		
	Conventional SPECT	IQSPECT	Correlation coefficient	Conventional SPECT	IQSPECT	Correlation coefficient
EDV [ml]	66.6±21.6	66.4±20.0	0.961	71.4±19.0	69.1±19.1	0.966
ESV [ml]	25.5±15.0	23.0±14.1	0.975	32.9±16.2	27.5±14.2	0.911
LVEF [%]	64.8±11.8	68.3±12.1	0.960	56.0±11.7	61.5±12.2	0.888

Mean±SD

**Figure 3.** Bland-Altman analysis of the segmental percent uptake on IQ-SPECT and conventional SPECT in ²⁰¹Tl studies. a) apex, b) anterior, c) septal, d) lateral, and e) inferior. The mean difference in the lateral wall between IQ-SPECT and conventional SPECT slightly increased

tetrofosmin studies were 0.961 (EDV), 0.975 (ESV), and 0.960 (LVEF). For the ²⁰¹Tl SPECT, these values were 0.966, 0.911, and 0.888, respectively (Table 3).

These parameters were not significantly different between IQ-SPECT and conventional SPECT. Although the mean ESV of IQ-SPECT tended to be slightly lower than that observed in conventional SPECT, none of the parameters were significantly different between IQ-SPECT and conventional SPECT (^{99m}Tc-tetrofosmin, $p=0.614$; ²⁰¹Tl, $p=0.174$). The mean differences of ESV in the ^{99m}Tc-tetrofosmin SPECT were 0.2 ± 6.0 ml (EDV) and 2.4 ± 3.3 ml. For the ²⁰¹Tl studies, these values were 2.3 ± 5.0 ml and 5.3 ± 6.7 ml, respectively (Figure 5).

The LVEF values of IQ-SPECT and conventional SPECT showed significant

correlations with respect to ^{99m}Tc-tetrofosmin and ²⁰¹Tl protocols. Although the mean LVEF of IQ-SPECT tended to be higher than that observed in conventional SPECT, the difference was not significant (^{99m}Tc-tetrofosmin, $P=0.269$; ²⁰¹Tl, $p=0.069$). The mean differences measured in the Bland-Altman analysis were $-3.5 \pm 3.4\%$ (^{99m}Tc-tetrofosmin) and $-5.5 \pm 5.7\%$ (²⁰¹Tl) (Figure 5).

Discussion

In this study, we evaluated the concordance of MPI images between on IQ-SPECT versus conventional SPECT using ^{99m}Tc-tetrofosmin and ²⁰¹Tl protocols. The segmental percent uptake exhibited a significant correlation ($P<0.05$) between IQ-SPECT and conventional SPECT; the mean difference was approximately zero in the Bland-Altman analysis. In addition,

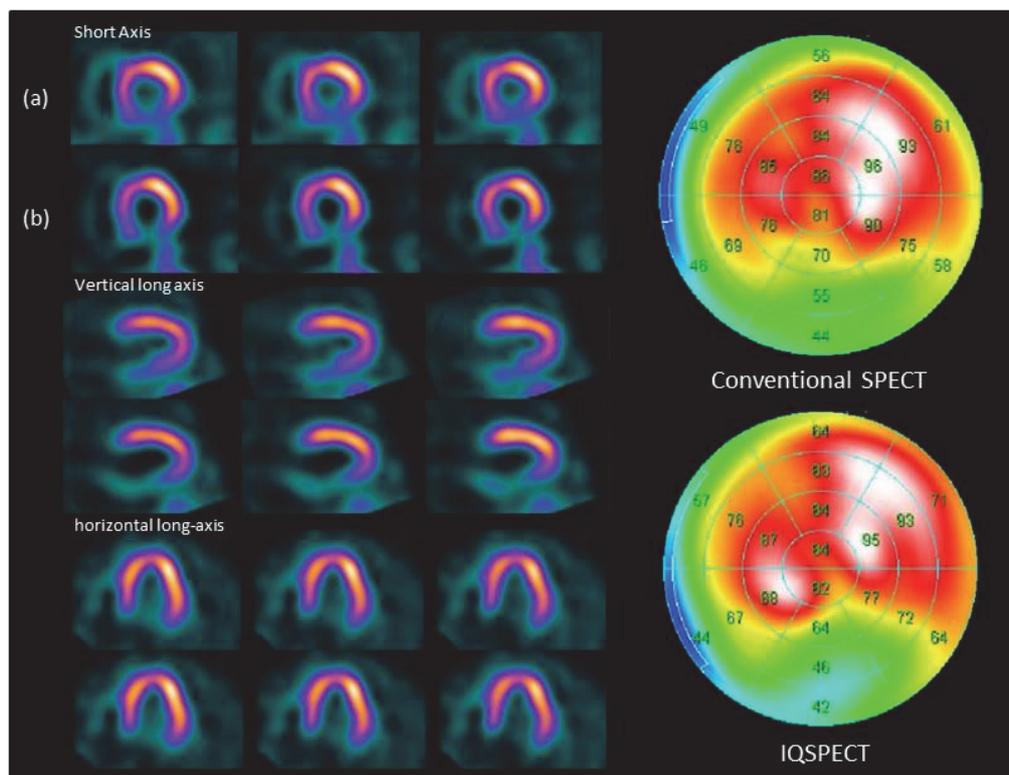


Figure 4. ^{99m}Tc -tetrofosmin MPI SPECT of a 74-year-old male with an old myocardial infarction in the inferobasal wall. Both IQ-SPECT and conventional SPECT show perfusion defect in the inferobasal wall; (a) conventional SPECT, (b) IQ-SPECT

quantitative parameters (EDV, ESV, and LVEF) were not significantly different between IQ-SPECT and conventional SPECT. Our results indicate that image accuracy and reproducibility of IQ-SPECT with a short acquisition time are similar to those of conventional MPI SPECT.

Regarding the segmental percent uptake, the lateral wall uptakes tended to be lower in IQ-SPECT compared to conventional SPECT. IQ-SPECT employs cardio-centric acquisition, and the acquisition angle is limited to a 208° arc. Bax et al. (13) and Go et al. (14) observed that enhanced image contrast with narrow acquisition results in geometric image distortion. In addition, Liu et al. (15) reported that a narrow acquisition orbit (e.g., 180° acquisition) yields a higher image contrast, compared to 360° acquisition in reconstructed images; in particular, the target objects are off-set on the field of view.

Our results demonstrated a similar tendency to the previously described effects due to the use of acquisition orbits. However, the differences between IQ-SPECT and conventional SPECT were slightly less significant in this study, and there were no significant differences in the level of segmental uptake. We conclude that the differential segmental uptake caused by the acquisition orbits does not affect image uniformity or homogeneity.

We also found that the LV volume (EDV and ESV) of IQ-SPECT was very similar to that observed in conventional SPECT. However, the mean LVEF of IQ-SPECT was slightly higher than that of conventional SPECT images in Bland-Altman plot. This finding demonstrates the higher image resolution of IQ-SPECT, compared to conventional SPECT.

Similarly, Onishi et al. (11) reported that the use of IQ-SPECT is more effective than conventional SPECT in terms of improving image resolution. The IQ-SPECT reconstruction method employs an iterative reconstruction algorithm with resolution recovery and a collimator geometric response function. Therefore, the application of resolution recovery algorithm reduces the partial volume effect, which seems to result in an increase in image contrast (16, 17). Despite the improvement of image contrast observed in IQ-SPECT, the increase in LVEF is insignificant and does not influence the diagnosis.

We compared the efficacy of IQ-SPECT, using a short acquisition time, with that of conventional SPECT, employing a standard acquisition time. Our results showed that accuracy and reproducibility of IQ-SPECT with a short acquisition time is similar to that observed in conventional SPECT.

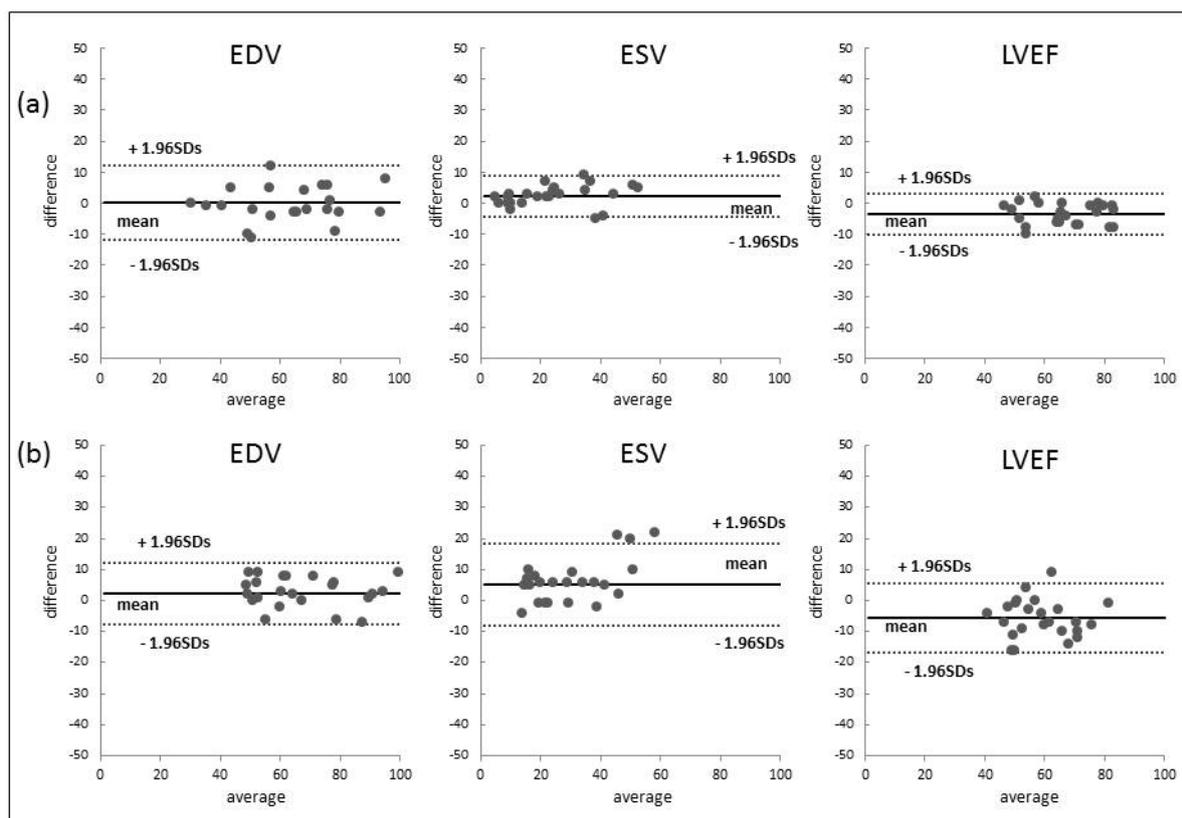


Figure 5. Bland-Altman analysis of the LV volume and ejection fraction on IQ-SPECT and conventional SPECT; (a) ^{99m}Tc -tetrofosmin study, (b) ^{201}Tl study. The mean ESV on IQ-SPECT was lower than that observed on conventional SPECT. In addition, there was a trend toward a higher mean LVEF on IQ-SPECT, compared to conventional SPECT

In general, the SPECT protocol is determined according to the trade-off between image acquisition time and noise level. Laetitia et al. (18) showed that IQ-SPECT increases the photon sensitivity and contrast-noise ratio more than conventional SPECT. Ali et al. (19) demonstrated that the application of reconstruction algorithm with resolution recovery reduces the acquisition time, although the diagnostic accuracy remains the same. Our results also showed that the use of IQ-SPECT reduces the acquisition time, required for ^{201}Tl studies.

The long effective half-life of ^{201}Tl limits the dose that can be injected. Therefore, ^{201}Tl studies usually require a long acquisition time in order to secure sufficient image quality in comparison with ^{99m}Tc studies. Furthermore, we performed conventional SPECT using a triple-head gamma camera. Although these cameras exhibit higher sensitivity compared to dual-head cameras, the IQ-SPECT protocol in MPI required a shorter acquisition time compared to conventional SPECT, using a triple-head camera. Our results suggest that the application of IQ-SPECT also confers advantages with regard to patient comfort, and potentially reduces patient motion. Moreover, this technique may also offer

the opportunity to reduce the injected dose to the patient.

There are several limitations inherent in this study. Firstly, in order to avoid introducing additional variation from system-specific correction methods, neither scatter nor attenuation correction was performed. Compton scattering and photon absorption are particularly important factors since organs of significantly different densities (20) surround the heart.

Viji et al. (21) reported that energy-window-based scatter estimate and CT-based attenuation correction are included in IQ-SPECT. Therefore, the use of scatter and attenuation correction may result in different performance outcomes with respect to the level of quantitative segmental tracer uptake. Therefore, further studies are required to examine image quality with attenuation and scatter correction.

Secondly, this study only examined the efficacy of rest MPI SPECT. Patient and/or organ motion such as upward creeping of the heart is often observed after exercise stress (22), and such motions during image acquisition can lead to serious reconstruction artifacts. Finally, no assessment of diagnostic accuracy was performed, although evaluation of diagnostic

accuracy is necessary for determining the clinical usefulness of IQ-SPECT.

Conclusion

In this study, IQ-SPECT with shorter acquisition time provided MPI SPECT images, comparable to those of conventional SPECT, using a triple-head gamma camera, according to ^{99m}Tc and ^{201}Tl protocols. Our results suggest that IQ-SPECT is a beneficial technology for performing MPI SPECT, and this modality is expected to increase scan efficiency and improve patient comfort.

References

- DePuey EG, Ernest VG. Updated imaging guidelines for nuclear cardiology procedures. *J Nucl Cardiol.* 2001; 8: G1-G58.
- Klocke FJ, Baird MG, Lorell BH, Bateman TM, Messer JV, Berman DS, et al. ACC/AHA/ASNC guidelines for the clinical use of cardiac radionuclide imaging—executive summary report of the American College of Cardiology/American Heart Association Task Force on Practice Guidelines (ACC/AHA/ASNC Committee to Revise the 1995 Guidelines for the Clinical Use of Cardiac Radionuclide Imaging. *J Am Coll Cardiol.* 2003; 42: 1318-33.
- DePasquale EE, Nody AC, DePuey EG, Garcia EV, Pilcher G, Bredlau C, et al. Quantitative rotational thallium-201 tomography for identifying and localizing coronary artery disease. *Circulation.* 1988; 77: 316-27.
- Thomas GS, Miyamoto MI, Morello AP, Majmundar H, Thomas JJ, Sampson CH, et al. Technetium-99m sestamibi myocardial perfusion imaging predicts clinical outcome in the community outpatient setting—The Nuclear Utility in the Community (NUC) Study. *J Am Coll Cardiol.* 2004; 43: 213-23.
- Nishimura T, Nakajima K, Kusuoka H, Yamashina A, Nishimura S. Prognostic study of risk stratification among Japanese patients with ischemic heart disease using gated myocardial perfusion SPECT: J-ACCESS study. *Eur J Nucl Med Mol Imaging.* 2008; 35: 319-28.
- Asao K, Takaki A, Tominaga M, Sasaki M. The interpolated projection data estimation method improves the image quality of myocardial perfusion SPECT with a short acquisition time. *Ann Nucl Med.* 2012; 26:123-30.
- Borges-Neto S, Pagnanelli RA, Shaw LK, Honeycutt E, Shwartz SC, Adams GL, et al. Clinical results of a novel wide beam reconstruction method for shortening scan time of Tc-99m cardiac SPECT perfusion studies. *J Nucl Cardiol.* 2007; 14: 555-65.
- Sun XX, Tian YQ, Wang DY, He ZX. Shortened acquisition time or reduced-activity dose for gated myocardial perfusion SPECT with new reconstruction algorithm. *Int J Cardiovasc Imaging.* 2013; 29:1287-93.
- Venero CV, Heller GV, Bateman TM, McGhie A, Ahlberg AW, Katten D, et al. A multicenter evaluation of a new post-processing method with depth-dependent collimator resolution applied to full-time and half-time acquisitions without and with simultaneously acquired attenuation correction. *J Nucl Cardiol.* 2009; 16: 714-25.
- DePuey EG. Advances in SPECT camera software and hardware: Currently available and new on the horizon. *J Nucl Cardiol.* 2012; 19: 551-81.
- Onishi H, Matsutomo N, Kangai Y, Saho T, Amijima H. Differential impact of multi-focus fan beam collimation with L-mode and conventional systems on the accuracy of myocardial perfusion imaging: Quantitative evaluation using phantoms. *Asia Oceania J Nucl Med.* 2013; 1: 28-34.
- Germano G, Erel J, Lewin H, Kavanagh PB, Berman DS. Automatic quantitation of regional myocardial wall motion and thickening from gated technetium-99m sestamibi myocardial perfusion single-photon emission computed tomography. *J Am Coll Cardiol.* 1997; 30: 1360-7.
- Bax JJ, Visser FC, van Lingen A, Sloof GW, Cornel JH, Visser CA. Comparison between 360 and 180 data sampling in thallium-201 rest-redistribution single-photon emission tomography to predict functional recovery after revascularization. *Eur J Nucl Med.* 1997; 24: 516-22.
- Go RT, MacIntyre WJ, Houser TS, Pantoja M, O'DENNEL JK, Feiglin DH, et al. Clinical evaluation of 360 and 180 data sampling techniques for transaxial SPECT thallium-201 myocardial perfusion imaging. *J Nucl Med.* 1985; 26: 695-706.
- Liu YH, Lam PT, Sinusas AJ, Frans JT. Differential effect of 180 and 360 acquisition orbits on the accuracy of SPECT imaging: quantitative evaluation in phantoms. *J Nucl Med.* 2002; 43: 1115-24.
- Hughes T, Celler A. A multivendor phantom study comparing the image quality produced from three state-of-the-art SPECT-CT systems. *Nucl Med Commun.* 2012; 33: 663-70.
- Onishi H, Motomura N, Fujino K, Natsume T, Haramoto Y. Quantitative performance of advanced resolution recovery strategies on SPECT images: evaluation with use of digital phantom models. *Radiol Phys Technol.* 2013; 6: 42-53.
- Imbert L, Poussier S, Franken PR, Songy B, Verger A, Morel O, et al. Compared performance of high-sensitivity cameras dedicated to myocardial perfusion SPECT: a comprehensive analysis of phantom and human images. *J Nucl Med.* 2012; 53: 1897-903.
- Ali I, Ruddy TD, Almgrahi A, Anstett FG, Wells RG. Half-time SPECT myocardial perfusion imaging with attenuation correction. *J Nucl Med.* 2009; 50: 554-62.

20. Hendel RC, Berman DS, Cullom SJ, Follansbee W, Heller GV, Kiat H, et al. Multicenter clinical trial to evaluate the efficacy of correction for photon attenuation and scatter in SPECT myocardial perfusion imaging. *Circulation*. 1999; 99: 2742-9.
21. Vija AH, Malmin R, Yahil A, Zeintl J, Bhattacharya M, Rempel TD, et al. A method for improving the efficiency of myocardial perfusion imaging using conventional SPECT and SPECT/CT imaging systems. Paper represented at IEEE Nuclear Science Symposium conference. 2010; 6: 3433-7.
22. Germano G. Technical Aspects of Myocardial SPECT Imaging. *J Nucl Med*. 2001; 42: 1499-1507.